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B_1^+ Phase Retrieval for Non-Quadrature Radio Frequency Excitation and Its Preliminary Application in MR-EPT

Gokhan Ariturk¹ and Yusuf Ziya Ider^{1,2}

Abstract

Non-quadrature radio frequency (RF) excitation has been widely studied in the fields of RF shimming, local SAR estimation, and MR-EPT with the use of multi-channel transceiver arrays. These studies generally require the retrieval of the complex transmit field (B_1^+), which can be accomplished by acquiring its magnitude and phase in different steps. Magnitude of the transmit field is acquired with the conventional methods which give accurate results for both quadrature and non-quadrature excitations. On the other hand, there is no straightforward method to acquire the absolute phase of the transmit field and generally approximations in MRI experiments are made in order to get it. However, many of these approximations fail in non-quadrature excitation and/or in ultra high fields. In this study, we propose a simple method to acquire the absolute transmit phase in non-quadrature excitation with an eight channel transceiver TEM array for 3 T. The proposed method requires the application of a single additional quadrature drive in order to get the receive phases of the individual channels of the transceiver coil. These receive phases are then subtracted from the transceiver phase of the non-quadrature drive experiment to acquire its transmit phase. The developed ideas are tested in the framework of simulations and MRI experiments with the use of four different non-quadrature drive configurations. It has been observed that the simulated and experimentally acquired transmit phase distributions tend to have a strong consensus which supports the validity of the proposed method. Finally, the estimated transmit phase distribution of non-quadrature drive is used in the standard MR-EPT study to get the conductivity reconstructions in order for the validation of its eligibility in MR-EPT studies. **Keywords:** B_1^+ Phase Acquisition, TEM Transceiver Array, Non-Quadrature Excitation, B_1 Shimming, MR-EPT, Multichannel RF Transmission

1 Introduction

Throughout the advancements on multichannel transmit arrays in magnetic resonance imaging (MRI), non-quadrature radio frequency (RF) excitation has been ubiquitously studied in the fields of RF shimming, local specific absorption rate (SAR) estimation, and magnetic resonance electrical properties tomography (MR-EPT) [1–7]. For many of these studies, acquisition of the complex-valued transmit field ($B_1^+ = (B_x + iB_y)/2$) is crucial. In the studies of SAR determination, the complex B_1^+ field is used in the derivation of the necessary electric field components [1, 6, 7]. Especially in the studies, where the non-quadrature excitation is used to focus the transmit field on a particular location, calculation of SAR is even more problematic as assumptions on transmit phase estimation become less valid [1, 8, 9]. For the MR-EPT studies in which non-quadrature drive can be required such as in [10, 11], acquisition of the transmit phase serves as a backbone for the determination of the desired electrical property maps.

Retrieval of the complex B_1^+ is traditionally accomplished by acquiring its magnitude and phase in different steps. While there exists conventionally settled methods for obtaining the magnitude of B_1^+ for both quadrature and non-quadrature excitation [12–14], there is no straightforward method to obtain the *absolute* phase of the transmit field. Although there are studies to calculate the derivatives of the absolute transmit phases, which can also be used to determine the electrical property (EP) maps [8, 11, 15], a conventional method to estimate the *absolute* transmit phase is still the subject of many inquiries.

One of the most common methods for obtaining the phase of the transmit field is the transceiver phase approximation (TPA) which assumes that the transmit and receive phase distributions are equivalent and therefore half of the acquired transceiver phase is used as the transmit phase [5, 16]. TPA works best for the cases of quadrature excitation and quadrature reception with a birdcage or transverse electromagnetic (TEM) coil, when the static magnetic field strength is lower than or equal to 3 T [5, 16].

In non-quadrature excitation, however, TPA fails [8, 9] and there are different methods to estimate the absolute transmit phase such as in [1, 17]. In [1], differences in the electric properties reconstructed from different transmit elements are related to the gradient of a reference phase (e.g. receive phase of a particular receive element). Polynomial approximation is then made for the reference phase distribution and the polynomial coefficients are estimated by solving (with regularization) the linear equation system relating the aforementioned differences to the coefficients and the B_1^+ magnitude maps. Once the reference phase distribution is obtained, absolute transmit phases of all channels are found from the measured relative phase information. In [17], the absolute transmit phase derivatives

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are estimated by solving a set of equations for each pixel making use of the proton density corrected estimates of B_1^- ($B_1^- = (B_x - iB_y)^*/2$) as well as B_1^+ maps for each channel and Gauss's Law for magnetism ($\nabla \cdot \mathbf{B} = 0$). The absolute phase distribution is then obtained by integrating its gradient. In [1] and [17], since the method chosen for EP reconstruction assumes negligible gradients of the EPs, phase estimation near tissue boundaries can become less reliable. In [8], concepts similar to the ones in [1, 17] are used, and it is shown that gradient of absolute transmit phase for all channels can be obtained from measured relative phases and the B_1^+ maps only. Finally, in the EPT approaches [11, 15], a similar formulation is derived whereby the spatial derivatives of the absolute transmit phase can be estimated, this time without assuming negligible gradients of the EPs. In [8, 11, 15] the absolute phase can also be derived by integration, starting from a seed point. However, these methods require many transmit-receive experiments.

In this study, we propose a simpler method to determine the phase of the transmit field in an eight port microstrip transceiver TEM array for the case of non-quadrature excitation in 3 T. The proposed method requires a single additional quadrature driven MRI experiment. The developed ideas are tested in the framework of simulations and MRI experiments with the use of four different non-quadrature drive configurations. It has been observed that the simulated and experimentally acquired transmit phase distributions tend to have a strong consensus which supports the validity of the proposed method. Finally, the estimated transmit phase distribution of non-quadrature drive is used in the Helmholtz's equation based standard MR-EPT [18] to get the conductivity reconstructions in order for the validation of its eligibility in MR-EPT studies.

2 Theory

Commencing with the theory of the accumulated phase on a single channel of the TEM array in a sequence execution, the step-by-step transmit phase retrieval procedure for quadrature and non-quadrature drive are given in the following sections.

2.1 Accumulated Phase On a Single Channel of the TEM Array

The phase value at location \mathbf{r} on the MRI image, being acquired with the k^{th} channel where $k \in \{1, 2, 3, \dots, 8\}$ can be expressed as: [9, 16]

$$\Phi_k(\mathbf{r}) = \phi_{B_1^-}(\mathbf{r}) + \phi_{B_1^+}(\mathbf{r}) + \phi_{(0,k)} + \phi_{\Delta B_0}(\mathbf{r}) + \phi_{res}(\mathbf{r}) \quad (1)$$

where $\phi_{B_1^-}(\mathbf{r})$ is the receive phase of the k^{th} channel, $\phi_{B_1^+}(\mathbf{r})$ is the phase of the transmit field when either all of the channels or only some channels are transmitting, and $\phi_{(0,k)}$ is the position independent zero-order phase offset of the k^{th} channel being dependent on the connecting cable lengths, phase response of the receive amplifiers, and the spatial position of the receiver channel on the circular structure of the coil. The last two terms in equation (1), $\phi_{\Delta B_0}(\mathbf{r})$ and $\phi_{res}(\mathbf{r})$ are the phase contribution due to B_0 and eddy currents respectively. Their effect will be neglected in our studies assuming that the the Balanced Steady State Free Precession (bSSFP) sequence is used [5].

2.2 Quadrature Drive B_1^+ Phase Retrieval

In order to obtain the circularly polarized B_1^+ field, imitating the field in a quadrature driven birdcage coil (from two ports), the eight-channel TEM coil array is driven with phase increments of 45° among adjacent channels. This 8-channel drive configuration of the TEM array is also referred to as the ‘‘quadrature drive’’ in the context of this study. To retrieve the transmit phase in this configuration, we propose the use of transceive phase approximation (TPA). However, the eight receive phases from eight channels need to be merged to converge on a single volume receive phase in order for the proper use of the TPA.

In the quadrature drive, the eight channel TEM array can also be used as a birdcage-like volume receive coil if during reception, the signals acquired from different channels are combined with proper phase increments [9]. These ‘‘proper’’ phase increments are required to eliminate the zero-order phase term ($\phi_{(0,k)}$) in equation (1).

For quadrature excitation, the transceive phase of the volume coil configuration ($\phi_{B_1^{trc}}^{quad}(\mathbf{r})$) for an 8 channel TEM array can be calculated from the MRI images obtained from individual receive channels as in equation (2):

$$\phi_{B_1^{trc}}^{quad}(\mathbf{r}) = \arg\left(\sum_{k=1}^8 p_k(\mathbf{r})e^{i(-\phi_{(0,k)})}\right) \quad (2)$$

where $p_k(\mathbf{r})$ is the complex MRI image pixel value at location \mathbf{r} which is obtained with the k^{th} receive channel. Moreover, $\phi_{(0,k)}$ is the zero order phase offset of the k^{th} channel, being mentioned in equation (1). Ideally, if the phase responses of the RF pre-amplifiers and receive cable lengths were precisely equivalent, this zero-order phase would have only been dependent on the spatial position of the receive channel and attain a value of 45° among adjacent channels. However, additional phase increments due to hand-made receive pre-amplifiers turn out to be different, and therefore, estimating this additional phase offset is accomplished by averaging the phase of a small

region of interest (ROI) in the middle of the phantom with equation (3), as used in [9].

$$\phi_{(0,k)} \simeq \arg\left(\sum_{roi} \frac{p_k(\mathbf{r})}{|p_k(\mathbf{r})|}\right) \quad (3)$$

Approximation of the zero-order phase terms of k^{th} channel in equation (3) originates from the theory that the transceive phases acquired from each channel need to attain the same value in the middle of an EP-wise symmetrical phantom [9]. Equation (2) makes the zero-order phase term correction by arbitrarily setting the averaged phases at the center of the phantom to zero for all of the channels. With the offset-corrected volume transceive phase in equation (2), the volume transmit phase is approximated by the transceive phase approximation as in the following:

$$\phi_{B_1^+}^{quad}(\mathbf{r}) = \phi_{B_1^{trc}}^{quad}(\mathbf{r})/2 \quad (4)$$

2.3 Non-Quadrature Drive B_1^+ Phase Retrieval

After acquiring the TPA approximated transmit phase using the above procedure, as a by-product, the offset corrected receive phase of the k^{th} channel can be calculated as:

$$\phi_{B_1^+}^{-*}(\mathbf{r}) = \arg\left\{\frac{\exp\left(i\phi_{B_1^{trc}}^{quad}(\mathbf{r})\right)}{\exp\left(i\phi_{B_1^+}^{quad}(\mathbf{r})\right)}\right\} \quad (5)$$

where $\phi_{B_1^{trc}}^{quad}(\mathbf{r})$ is the transceive phase, retrieved with the k^{th} channel during the quadrature drive and $\phi_{B_1^+}^{quad}(\mathbf{r})$ is the quadrature drive volume transmit phase obtained with equation (4). These receive phases are specific for each receive channel and will be equivalent in quadrature and non-quadrature drive experiments.

The volume transmit phase of the non-quadrature drive ($\phi_{B_1^+}^{non-quad}(\mathbf{r})$) can be calculated using one of the receive channels with the following formula:

$$\phi_{B_1^+}^{non-quad}(\mathbf{r}) = \arg\left\{\frac{\exp\left(i\phi_{B_1^{trc}}^{non-quad}(\mathbf{r})\right)}{\exp\left(i\phi_{B_1^+}^{-*}(\mathbf{r})\right)\exp\left(i\phi_{(0,k)}\right)}\right\} \quad (6)$$

where $\phi_{B_1^{trc}}^{non-quad}(\mathbf{r})$ is the transceive phase acquired from the k^{th} channel during the non-quadrature drive. It should be noticed that the same zero-order phases, which were calculated in the quadrature drive are used in equation (6) for offset correction. It is expected that equation (6) would yield the same result, irrespective of the channel being used, i.e., same result for every channel. Therefore, the average of the transmit phases, being found from eight channels can also be used.

3 Methods

3.1 Simulations and RF Inputs for Non-Quadrature Drive

Finite Element Method (FEM) based simulations in Comsol Multiphysics® (COMSOL AB, Stockholm, Sweden) were performed not only for having a comparison between the simulated and experimentally acquired transmit phase, but also for calculating the RF inputs of the TEM array in non-quadrature drive.

Simulation model of the eight port TEM array, being depicted in figure (1a) is extensively given in [10]. This decoupled coil array has a radius of 15 cm (from the center to the middle of each microstrip line element) and a length of 30 cm. Microstrip lengths and widths of each line element are given as 27 cm and 2 cm. The dielectric material between microstrip conductors is chosen as plexiglass with a thickness of 1 cm and a relative dielectric constant of $\epsilon_r = 3.6$ to have a characteristic impedance of approximately 50 Ω . Matching, tuning and decoupling capacitors are depicted with their capacitance values in figure (1a). The cylindrical simulation phantom, having a background conductivity of 0.5 S/m and two cylindrical anomalies with $\sigma = 1$ S/m is shown in figure (1b). Outer radius of the phantom is given as 8 cm and the radii of each anomaly are 1.5 cm. The relative permittivity and permeability values in the entire phantom are given as $\epsilon_r = 80$ and $\mu_r = 1$, respectively.

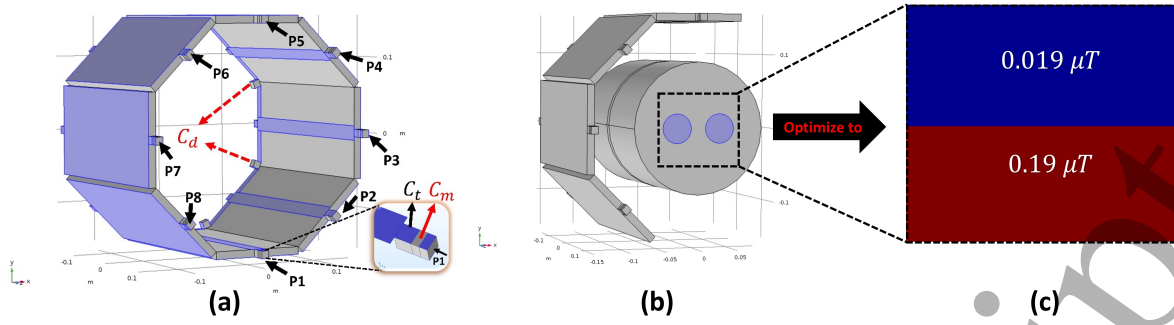


Figure 1: (a): Simulation model of the empty eight-channel TEM array. C_m is the matching, C_t is the tuning and C_d is the decoupling capacitor with 2.5 pF, 31.5 pF and 1 pF capacitances, respectively. (b): Cylindrical simulation phantom with two cylindrical anomalies, shown inside the coil. Background conductivity is 0.5 S/m and the conductivities inside the anomalies are 1 S/m each. (c): The optimization goal distribution ($\mathbf{B1}^{+,goal}$).

RF inputs for the non-quadrature drive are found by optimizing the phases of RF input signals ($\phi_{RF1}, \phi_{RF2}, \dots, \phi_{RF8}$) applied from the ports of the TEM array, such that the magnitude of the constructed B_1^+ distribution in a square shaped ROI (shown in figure (1b)) is similar to the desired discrete B_1^+ distribution, $\mathbf{B1}^{+,goal}$ (depicted in figure (1c)). This method is similar to the ones in [4, 7], however, only the phases of the input RF signals are optimized as in [19] (same magnitude for every channel). It can be seen that $\mathbf{B1}^{+,goal}$ has a high field region, a low field region, and a sharp transition in the middle. $\mathbf{B1}^+(\theta)$ vector is the discretized version of the continuous B_1^+ field inside the coil and it is dependent on the RF input phase vector $\theta = [\phi_{RF1}, \phi_{RF2}, \dots, \phi_{RF8}]^T$. Using the superposition principle, $\mathbf{B1}^+(\theta)$ can be written as in the following:

$$\mathbf{B1}^+(\theta) = \sum_{n=1}^8 e^{i\phi_{RFn}} \mathbf{B1}^{n+}(1V, 0^\circ) \quad (7)$$

where $\mathbf{B1}^{n+}(1V, 0^\circ)$ represents the discretized B_1^+ distribution when all the channels except channel n is terminated with the reference impedance (50 Ω) and channel n is driven by 1 V RF amplitude and 0° phase offset. In this regard, the θ dependent cost function is given as:

$$C(\theta) = \sum_{i=1}^M (|B1_i^+(\theta)| - |B1_i^{+,goal}|)^2 \quad (8)$$

where $B1_i^{+,goal}$ and $B1_i^+(\theta)$ represent the i^{th} elements of the $\mathbf{B1}^{+,goal}$ and $\mathbf{B1}^+(\theta)$ vectors respectively. Furthermore, M denotes the total number of elements in each vector. The cost function is minimized with the steepest descent method of the “Optimization Toolbox” of Matlab[®] (Mathworks, Natick, USA) to get the input RF phases. As the top part of the $\mathbf{B1}^{+,goal}$ is the low field region, this is called as the “Top Shadowed” excitation configuration. The other non-quadrature drive configurations are its rotated versions and are called as the “Right”, “Left”, and “Top-Right” shadowed excitation configurations. Their RF input phases are demonstrated in table (1). It should be noted that the optimization procedure is applied for an EP-wise homogeneous phantom, where the anomalies in figure (1) have the same EP’s as in the background.

	ϕ_1	ϕ_2	ϕ_3	ϕ_4	ϕ_5	ϕ_6	ϕ_7	ϕ_8
Quad	0	45	90	135	180	225	270	315
Right Sh	46.22	133.19	-147.08	-54.38	26.39	19.33	19.41	-43.10
Top-Right Sh.	133.19	-147.08	-54.38	26.39	19.33	19.41	-43.10	46.22
Top Sh	-147.08	-54.38	26.39	19.33	19.41	-43.10	46.22	133.19
Left Sh	26.39	19.33	19.41	-43.10	46.23	133.19	-147.08	-54.38

Table 1: The RF input phases (in the unit of degrees) for the quadrature drive and the four non-quadrature drive configurations: Top Shadowed, Top-Right Shadowed, Right Shadowed and Left shadowed. These phases are used both in simulations and experiments.

3.2 MRI Experiments

3.2.1 Multichannel Microstrip TEM Array, RF Front End, and Experimental Phantom

The eight-channel TEM array, which was designed to operate at 123.2 MHz, is constructed at home and the PLA based white coil casing is produced by ArtıBoyut® (Ankara, Turkey) company. The complete experimental setup including the TEM array, RF switch, and the experimental phantom is depicted in figure (2).

The constructed coil has the same dimensions as the simulation model given in section (3.1). Capacitance values of the shunted tuning capacitors were designed to be 31 pF in simulations, however 27 pF capacitors are used at both ends of the coil. In parallel to the 27 pF capacitors on the back end of the coil, variable capacitors (Knowles Voltronics 1-23 pF Non-Magnetic 750 V Trimmer, Part Number: NMAJ25HV) are used for tuning. Furthermore, the same type of variable capacitors are used in series for impedance matching in the front part of the array. S-parameters of the loaded coil are measured with a network analyzer (Agilent ENA E5061A 300 kHz - 1.5 GHz) and are depicted in figure (2g). As it can be seen, all of the reflection coefficients ($S_{11}, S_{22}, \dots, S_{88}$) attain a value of approximately -40 dB at 123.23 MHz and the isolation of the ports are at -14 dB at the worst case, which is sufficient [20–22].

The coil is used with an eight-channel hand-made RF transmit-receive (TR) switch including the RF pre-amplifiers which were designed and fabricated in the National Magnetic Resonance Research Center (UMRAM) (Ankara, Turkey). The RF front-end is conceptually very similar to the one in [22], however it is designed for 3T MRI scanners. Gains of the receive pre-amplifiers are in the range of 21-24 dB at an input source power of -20 dBm and the noise figures are in the range of 1.3-1.6 dB. Transmit-receive isolation of all of the eight channels of the switch are less than -25 dB, which is acceptable. The complete RF front end, including the coil, is shown in figure (2).

Transmission and reception are accomplished with the aforementioned hand-made RF front end, which is driven with an eight channel transmitter array system of Siemens Tim Trio 3 T MRI scanner. The eight transmitter channels (1 master + 7 slave) of the scanner allows the user to scale the RF input magnitudes and adjust their phases. In the beginning of the experiments, the optimal operating frequency is approximately found as 123.23 MHz, which is compatible with the coil measurements. In a single experiment, the RF signal magnitude, which is the same for all channels, is optimized by the scanner. The transmit phases for quadrature and four non-quadrature excitations are the same as in the simulations and are shown in table (1).

The agar phantom is prepared in a cylindrical flask of radius 7 cm and a height of 20 cm. Within the phantom, two cylindrical anomalies of 1.5 cm radius are located 5 cm apart with respect to their centers. The phantom has a background of agar-saline solution with 20 gr/l agar, 2 gr/l $NaCl$, and 3 gr/l $CuSO_4$, and two equivalent cylindrical anomalies of saline solution with 6 gr/l of $NaCl$ and 3 gr/l $CuSO_4$ each. With these concentrations, the electrical conductivity is expected to be 0.5 S/m in the background and 1 S/m in the anomalies [23].

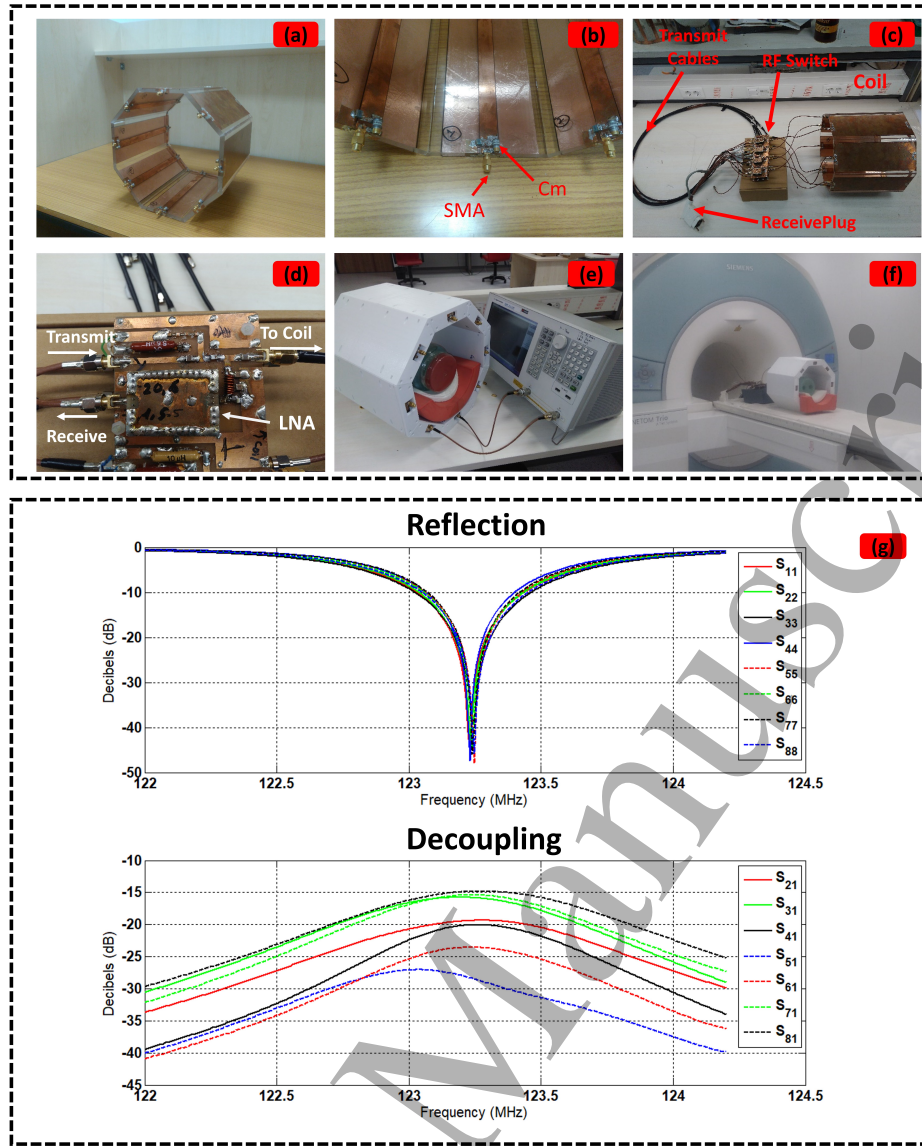


Figure 2: The complete RF front end including the RF coil, TR switch and connection cables. (a): Constructed 8 channel TEM array, being designed in [10]. (b): The bare coil viewed from front end. C_m is the matching capacitor. (c): The complete RF front end. (d): RF circuitry of the one channel of the TR switch, (e): The coil with casing, under measurements, (f): The complete experimental setup. (g): S-Parameters of the constructed coil. $S_{11}, S_{22} \dots S_{88}$ are the reflection coefficients and $S_{21}, S_{31} \dots S_{81}$, are used to measure the decoupling among channels.

3.2.2 MRI Sequences

For all of the experiments, magnitude of the transmit field ($|B_1^+|$) was found by the double angle method [12]. For each drive, two successive Gradient Recalled Echo (GRE) sequence executions with 60° and 120° flip angles were performed. The remaining parameters of the GRE sequences are: $FOV = 150$ mm, $TE/TR = (5 \text{ ms}) / (1500 \text{ ms})$, 2-D single slice with voxel size: $1.2 \times 1.2 \times 5$ mm, 2 averages. A single GRE execution takes approximately 6 minutes.

For the retrieval of the transceive phases, bSSFP sequence is used with the following parameters: $FOV = 150$ mm, $TE/TR = (2.34 \text{ ms}) / (4.68 \text{ ms})$, $FA = 40^\circ$, 2-D single slice with voxel size: $1.2 \times 1.2 \times 5$ mm, 256 averages (32 acquisitions \times 8 measurements). A single sequence execution takes approximately 2.5 minutes.

3.3 MR-EPT Method

The experimentally calculated transmit phase ($\phi_{B_1^+}$) is used in the Helmholtz's equation based standard (conventional) MR-EPT [18]. In this method, electrical conductivity (σ) is found by $\sigma = \text{Re}\{\frac{\nabla^2 H^+}{j\omega\mu_0 H^+}\}$ where $\omega = 2\pi f_0$, f_0 is the Larmor frequency, H^+ is the transmit field such that $H^+ = B_1^+/\mu_0$ and μ_0 is the permeability of free space.

3.4 Testing the Algorithm

As there is no straightforward algorithm to obtain the ground-truth absolute transmit phase, it was checked whether the experimentally estimated phase patterns comply with the following criteria or not.

1. The experimentally estimated transmit phase distribution needs to resemble the simulated ones,
2. Equation (6) should yield the same resultant volume transmit phase when the transceive phase for any of the eight channels is used.
3. Estimated transmit phase patterns of the non-quadrature excitation configurations need to comply with the “phase-incremented rotation” condition.

To understand the phase-incremented rotation condition, it needs to be recalled that the driving configurations of the non-quadrature drive cases are the rotated versions of each other. Therefore, the transmit phases of these excitation configurations also need to be the rotated versions of each other. Furthermore, a phase offset in the overall transmit phase should also be observed between two non-quadrature drive configurations [9]. For instance, the RF input pattern of Left Shadowed excitation is the circularly 180° rotated version of the input pattern of Right-Shadowed excitation, as depicted in figure (3). In this scenario, it is expected that the transmit phase pattern of Right Shadowed excitation is spatially 180° rotated and also 180° phase incremented version of the Left Shadowed drive, as also shown in figure (3). This condition is also verified in the experimental results with the addition of artificial phases.

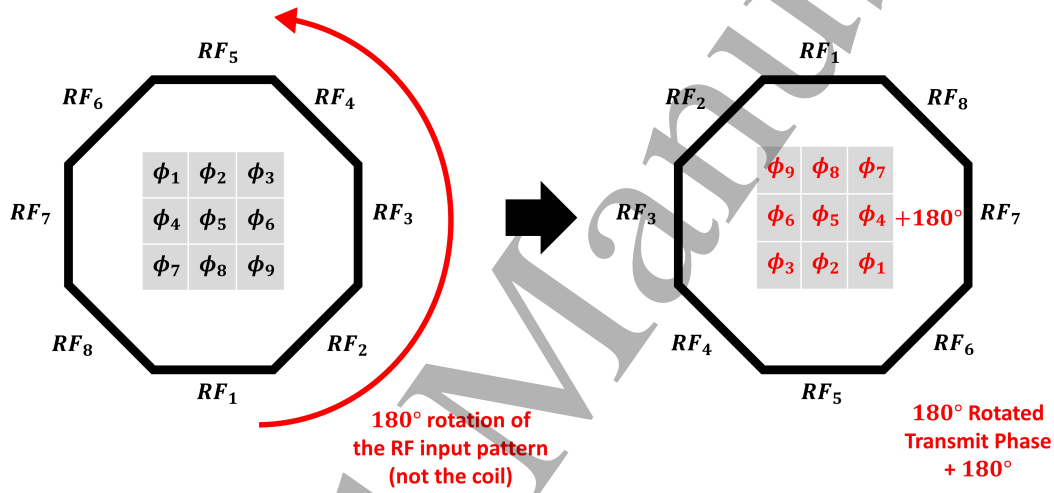


Figure 3: Phase-incremented rotation between two non-quadrature excitation configurations. If the RF input pattern (not the coil) is 180° rotated, the acquired transmit phase needs to be the 180° rotated and 180° phase incremented version of the previous drive.

4 Results

4.1 Receive and Non-Quadrature Transmit Phase Extractions

The experimental receive phases of each individual channel, being found in equation (5), are demonstrated in figure (4). As it can be seen, the receive phase distributions tend to have a rotational variation among adjacent channels.

Furthermore, the experimentally estimated transmit phase distributions of the Right-Shadowed drive, being calculated from each receive channel with equation (6) are also depicted on the same figure. As it can be seen, they are observed to be very similar. This strong similarity actually verifies the second condition of the testing criteria in the previous section. The transmit phase patterns of each channel for other non-quadrature cases are not included.

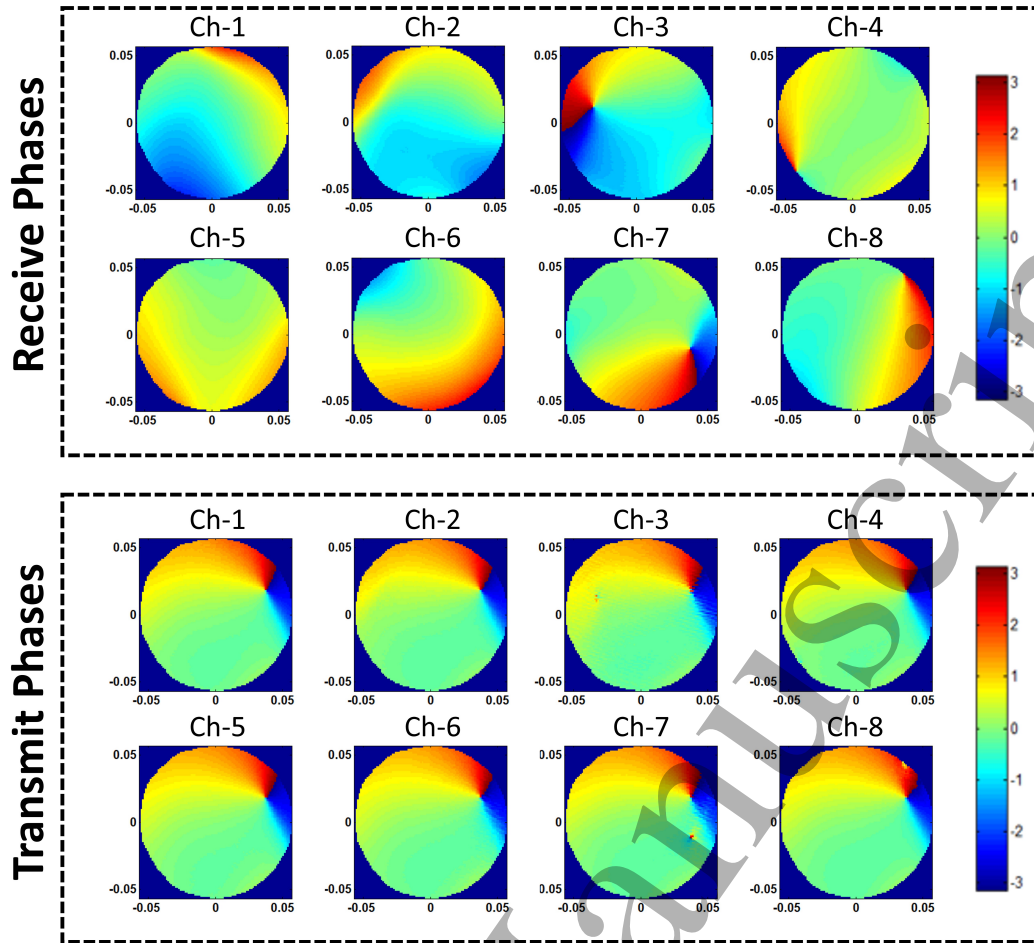


Figure 4: Experimental results: Receive phases of channels 1 to 8 (being found with equation (5)) are demonstrated in the upper box. In the lower one, the volume transmit phase distribution of the Right Shadowed excitation, being obtained from each channel, is depicted. For all of the images, horizontal axis is for $x(m)$ and vertical axis is for $y(m)$.

4.2 SSFP Magnitude, B_1^+ Magnitude and Phases

B_1^+ magnitude and B_1^+ phase images for the quadrature and also the non-quadrature (i.e. Top, Right, Left, Top-Right shadowed) drives are demonstrated in figure (5). That figure illustrates the results of both simulations and experiments. It should be noted that the result of the channel with the best SNR (estimated with equation (6)) is used in the experimental B_1^+ phase images. The experimental bSSFP magnitude images are also depicted on the same figure.

Considering the quadrature drive, it can be observed that the B_1^+ magnitude image has a central brightening pattern, both in simulations and experiments. This pattern is slightly disturbed by the conductive anomalies of the phantom. On the other hand, magnitude of the quadrature driven bSSFP image has increasing intensities at the top left and bottom right parts, due to different gains from hand-made receive pre-amplifiers.

Regarding the experimental transmit phase image of the quadrature drive in figure (5b), which was found by equation (4), a paraboloid shaped classical quadrature drive volume phase pattern is observed, being very similar to the simulated quadrature drive phase distribution in figure (5a).

Considering all of the non-quadrature drive configurations, the magnitude of the transmit fields in simulations and experiments turn out to be highly similar, as it can be seen in figure (5a) and (5b). For the experimental results, on the other hand, it is observed that the image quality is significantly reduced in the regions where B_1^+ magnitude is low (the “shadowed” regions), due to low signal to noise ratio (SNR) values.

The experimentally found non-quadrature transmit phase estimations, depicted in figure (5b) are also similar to the ones found in simulations, as shown in figure (5a). In the transmit phase patterns, large phase excursions, being located at the center of the regions where B_1^+ magnitude significantly drops, are observed as emphasized with the arrows in figure (5a) and (5b).

Evaluating the results shown in figure (5), it should be noticed that the B_1^+ phase extraction pattern resemblances between simulations and experiments are stronger for the quadrature excitation than the ones in non-quadrature drive

cases. One predominant reason for this issue can be suggested as the difference between simulated and experimental channel coupling performances. It was indeed observed in simulations that slight variations in channel coupling – when such asymmetrical non-quadrature excitations are employed – yield considerably different transmit phase patterns within the sample.

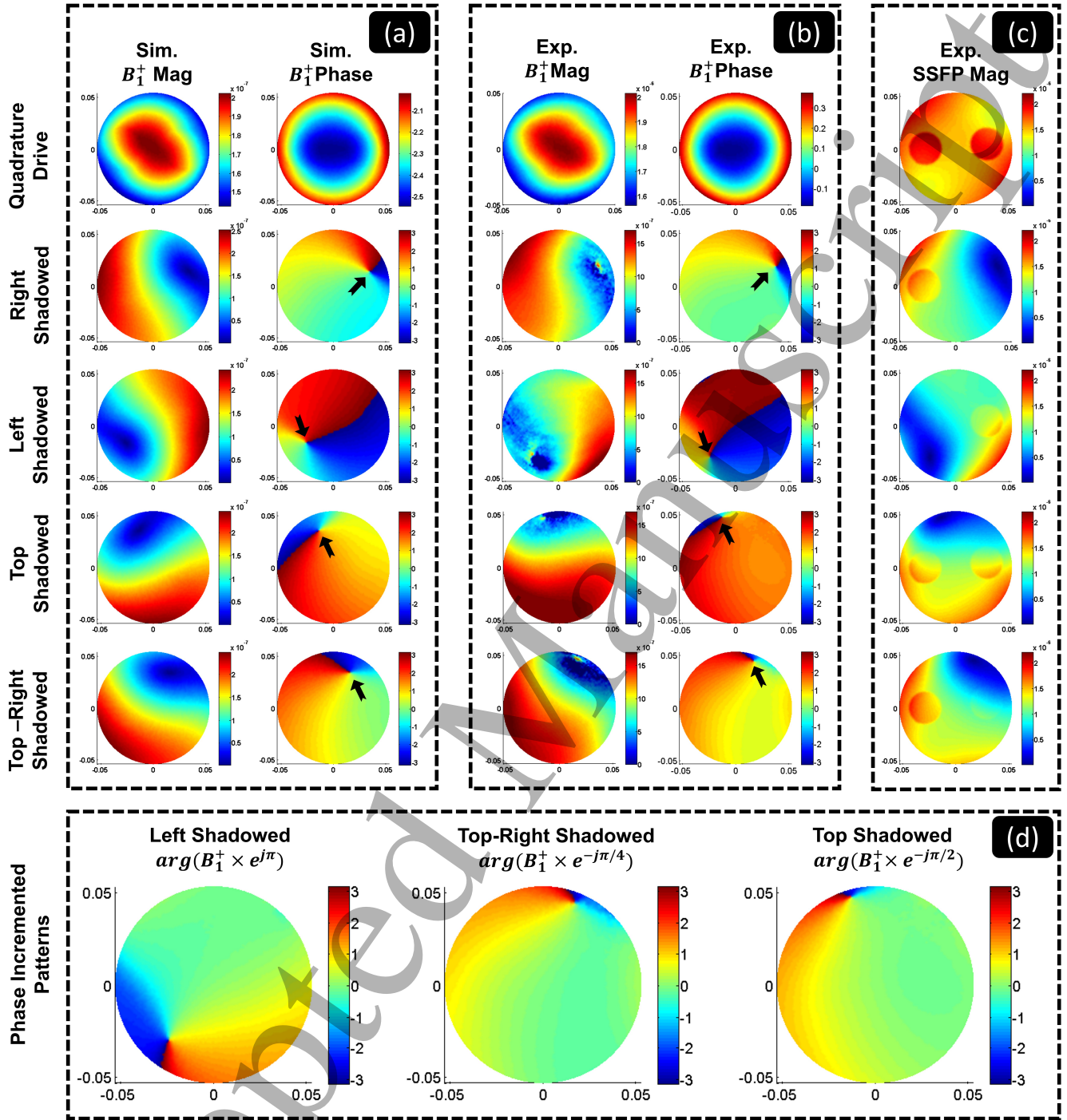


Figure 5: Comparison of the simulated and experimental results for the quadrature and four different non-quadrature drive configurations. (a): Simulated B_1^+ magnitude and phase distributions, (b): Experimental B_1^+ magnitude and experimental B_1^+ phase patterns, (c): Experimental bSSFP magnitude images, (d): Software-wise phase incremented versions of the experimentally estimated phase pattern of the left, top-right and top shadowed drive configurations to test the phase-incremented rotation condition. For all of the images, horizontal axis is for $x(m)$ and vertical axis is for $y(m)$.

In order to verify the phase-incremented rotation condition in MRI experiments, as described in section (4), proper phases are added to the experimentally acquired transmit phases in Left Shadowed, Top Shadowed and Top-Right Shadowed excitations to verify whether they imitate the rotated versions of the right shadowed one. When phase

offsets of 180° , -45° , and -90° are added to the Left, Top-Right, and Top Shadowed complex B_1^+ distributions, their phase patterns become very similar to the spatially 180° , -45° , and -90° rotated versions of the phase pattern of the Right-Shadowed configuration, as depicted in figure (5d).

The observed consensus between the experimental and simulation results and the compliance of the experimental results with the phase incremented rotation condition turn out to be two majorly important points in the assessment of the accuracy of the transmit phase estimations.

4.3 Conductivity Reconstructions

The experimental conductivity reconstructions obtained with the standard MR-EPT method for the quadrature drive and also for the two non-quadrature drive (top and right shadowed) configurations are shown in figure (6). As expected, the best conductivity reconstructions are obtained with the data of quadrature drive, as it has the best SNR values (figure (6a)). The artifacts along anomaly boundaries are typical of the standard MR-EPT method as it makes the Local Homogeneity Assumption (LHA). Otherwise, the background conductivity of 0.5 S/m and the conductivities of anomalies with 1 S/m are accurately reconstructed.

Among the two non-quadrature drive configurations, similar behavior in the conductivity reconstructions are observed. Regarding the distinguishability between background and anomalies, they have similar performance. However, the regions with low B_1^+ magnitude tend to be highly distorted, as expected. Furthermore, the overall image quality is also reduced compared to the quadrature drive conductivity reconstruction because of noise contamination in B_1^+ phase distributions, originating from the several steps of post-processing involved in extracting the non-quadrature transmit phases.

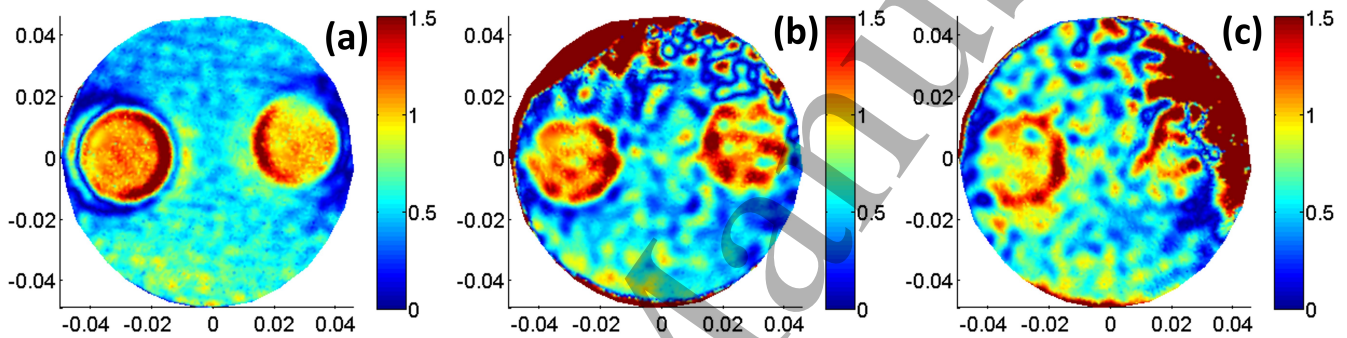


Figure 6: Experimental conductivity reconstructions: Standard MR-EPT reconstructions of the quadrature drive, top shadowed and right shadowed excitation configurations in (a),(b), and (c), respectively. For all of the images, horizontal axis is for $x(m)$ and vertical axis is for $y(m)$.

5 Conclusion and Discussion

Throughout this study, a simple and experimentally less demanding method to estimate the non-quadrature drive B_1^+ phase distribution has been proposed. The method is tested in the framework of simulations and MRI experiments. It is observed that the three significant points given in the criteria to evaluate the accuracy of phase estimations have been met. With the support of these three aspects, the proposed method is a nice candidate to be used in MR-EPT studies, as it requires only two B_1^+ magnitude and phase estimations which shortens the total MRI data acquisition time.

It should be pointed out, however, that computational procedures used throughout equation 1–7 decrease the SNR of the acquired data, hence, reducing the performance of the MR-EPT techniques. To acquire MRI images with higher SNR, the use of multichannel degenerate birdcage coil [24], receive-only loop arrays, or transceiver loop arrays [25] can be considered. Using receive-only loop coil arrays, the validity of TPA may become questionable and additional quadrature drive experiments can be needed to get the transmit phase of the transmitter coil [15]. On the other hand, use of wisely positioned loop arrays as transceiver antennas can provide higher SNR values within the periphery but lower SNR values at the central regions of the sample [25], latter being the main ROI in our studies. However, the overall SNR advantage of loop arrays (and degenerate birdcage coil) make them potentially feasible for use.

In addition to its use in MR-EPT studies, this method can also be used in the SAR estimation studies for finding the complex B_1^+ field distribution when non-quadrature excitation is employed.

Regarding the validity of TPA, it was argued in [26, 27] that the ratio between the axial dimensions of the sample and the RF wavelength is an important factor and that this ratio is acceptable for human head sized samples in 3T or lower systems. Since we also use a head-sized phantom and coil in a 3T system, the method proposed in our study for absolute transmit phase estimation should also have acceptable accuracy. On the other hand, use of ultra

high field systems ($> 3T$) and/or greater samples sizes (e.g. torso, pelvis, etc.) will result in discrepancies between transmit and receive phase patterns, especially at the non-central regions of the sample in quadrature drive, hence, reducing the accuracy of the approximated transmit phase pattern in those regions of the sample [26, 27].

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